The leads are still the weakest link

Jordan M. Prutkin, Arun R. Sridhar
Division of Cardiology, Section of Electrophysiology, University of Washington, Seattle, WA, United States

Since the invention of the first wearable pacemaker in 1958, the field of cardiac pacing has made a remarkable progress [2]. Much of the effort has gone into the improvement of generator longevity, size, and features. Lead development, on the other hand, has not been as much of a focus. Perhaps this is because operators and patients just expect leads to work. Leads form the vital connection through the vascular system to the heart and are subjected to immense amount of friction, inflammation, and fibrosis and the perpetual motion of the heart. Lead failures are much more common compared to generator and battery failures and pose management quandaries in terms of whether to abandon or extract them when implanting fresh leads [3].

The study by Dębski et al. [4] is a timely article which discusses the issue of lead longevity. The authors should be congratulated for their work. With data from 3771 patients over 30 years and a combined follow-up period of 24,432 patient-years, this study is one of the largest single-centre analyses of pacemaker lead-related complications. The authors studied three different lead dysfunctions: 1) lead dislodgement, 2) cardiac perforation, and 3) lead failure. The overall lead dysfunction rate was 5.5% of all leads, with the majority being lead failure (4.2%) followed by lead dislodgement (1.2%), and, rarely, cardiac perforation (0.1%)

LEAD DISLODGEMENT

Lead dislodgement occurred in 2.4% of the patients. The only independent predictor of dislodgement was implant in the atrial lead position. Other studies have similarly shown high dislodgement rates in the atrium. For instance, another study looking at both pacemakers and biventricular devices also showed that the right atrial lead had the highest rate of dislodgement (1.9%) followed by right ventricular (RV) implantable cardioverter-defibrillator lead (1.8%), coronary sinus lead (1.4%) and RV pacing lead (0.3%) [5].

The reason for the consistently high rates of atrial lead dislodgement is unclear. Intuitively, it appears that it could be because the atrial lead is essentially free floating, with less support compared to RV apical leads which are wedged into a narrow space at the apex. It may also be that the extendable helix may not screw as well into the myocardium when in a J-curve versus a straight line.

Unfortunately, the present study does not delve into the details of implant parameters. Ghani et al. [5] noted in their study that lead dislodgements could have been prevented by adequate fixation of suture sleeves in one-third of cases. Also, the current of injury at implantation has been shown to predict adequate fixation of leads, but this was not reported in the present study [6].

This study has significant strengths. The data are from a single well-experienced centre which reduces bias related to interoperator variability. There are also a low number of patients lost to follow-up, a large number of leads, a very
large total patient-years of follow-up, and a variety of leads studied over this period.

There are some important methodologic limitations to note in the study. Lead failure was defined as an elevated pacing threshold or sensing problems. However, not every change in pacing threshold or sensing abnormality is due to the lead. Physiological states such as electrolyte imbalances, hypoxia, hypop/hyperglycaemia, myocardial ischaemia and infarction, cardiomyopathy, certain medications, and endocrine disorders may all cause changes in sensing or threshold which are not lead malfunctions [8].

The authors do not differentiate between various modes of lead failure such as lead fracture or insulation breach. They also do not distinguish minor lead integrity issues which could be programmed around from catastrophic lead failure which would require a reoperation. For the patient and operator, this is probably the more important endpoint.

Lastly, this study only examined dual chamber systems and is not relevant to single chamber or biventricular systems which may have different lead-lead interactions or lead construction.

Therefore, there are several factors that underestimate or overestimate lead failure in this analysis.

Nevertheless, studies like this are helpful to inform patients about long-term risks, give insight about ways to improve lead placement by operators, instruct manufacturers about lead types and designs that are less effective in the long term, and provide post-market surveillance for regulatory agencies.

This study also emphasises the importance of continued development of leadless pacing systems, where there is no lead to fail. Only single chamber leadless pacemakers are currently available for routine use; and because of their novelty, we do not have long-term data for these devices. One-year follow-up of the Medtronic Micra and three-year follow-up of the Abbott Nanostim show promising stability of pacing and sensing parameters [9, 10], but there have been reports of premature battery failure with Nanostim [11] which will need to be corrected in later-generation devices.

In the near-term time horizon, we will likely use single chamber VDD and multicomponent dual chamber leadless pacemakers, as well as those which communicate with the subcutaneous implantable cardioverter-defibrillator [12]. Studies like this one from Dębski et al. [4] on transvenous pacemaker leads will hopefully be less needed. Leads continue to be the “weakest link” in the chain of cardiac pacing [13] but it appears that we are at the brink of the much-needed next revolution in cardiac pacing — a world without leads!

Conflict of interest: none declared

References